# ETSI TR 103 907 V1.1.1 (2024-08)



**Speech and multimedia Transmission Quality (STQ); Test methods for insert type headsets enabled with structure-borne speech capture** 

Reference

DTR/STQ-309

Keywords

bone conduction, headset, sound, speech, structure-borne, testing

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### Foreword

This Technical Report (TR) has been produced by ETSI Technical Committee Speech and multimedia Transmission Quality (STQ).

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### Introduction

As communication devices evolve to meet the demands of consumers and to enhance user experience, the integration of bone conduction technology into in-ear headsets allows significant advances in speech signal processing. Noise suppression and echo control functionalities utilize information of built-in bone conduction sensors inside the ear canal to better identify the talker's voice and separate it from possible degradations, like e.g. ambient noise or a concurrent talker.

However, standardized state-of-the-art test equipment is not able to simulate any transfer path between air-borne and structure-borne sound and thus, the actual performance of headsets cannot be adequately assessed. Recommendation ITU-T P.58 [\[i.1\]](#page-4-0), which specifies mouth simulator and usage of artificial ears of a HATS, even requires a rather high decoupling between both components. The present document introduces a modified version of standardized acoustic test equipment, which is able to overcome this limitation.

### <span id="page-4-0"></span>1 Scope

The present document provides test setups and test methods for headsets, which use human bone conduction as an additional input signal to the air-borne transmitted voice of the near-end talker. The work described in the present document includes test setup description, validation procedures and standardized test methods focusing on the timevariant behaviour of headset devices that utilize bone conduction in their signal processing.

### 2 References

#### 2.1 Normative references

Normative references are not applicable in the present document.

### 2.2 Informative references

References are either specific (identified by date of publication and/or edition number or version number) or non-specific. For specific references, only the cited version applies. For non-specific references, the latest version of the referenced document (including any amendments) applies.

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The following referenced documents are not necessary for the application of the present document but they assist the user with regard to a particular subject area.



### 3 Definition of terms, symbols, and abbreviations

### 3.1 Terms

For the purposes of the present document, the following terms apply:

**air-borne sound:** sound waves travelling through the air

**bone conduction:** sound conducted through the bones and tissue of the human skull

**structure-borne sound:** sound waves pulsating and radiating through a solid structure or medium (e.g. a human skull)

### <span id="page-5-0"></span>3.2 Symbols

Void.

### 3.3 Abbreviations

For the purposes of the present document, the following abbreviations apply:



### 4 Headset signal processing and potential improvements with bone conduction sensing

To define appropriate test methods, it is useful to have a look into areas where bone conduction signals may be used to improve the performance of headsets. The main purpose of using bone-conducted sound in signal processing is the improved separation between:

- near-end talker and near-end background noise;
- near-end talker and near-end concurrent talker;
- near-end talker and far-end talker (double talk detection).

A second benefit of using the bone conduction signal could be to directly transmit this signal instead of transmitting the near-end microphone signal, at least in the low frequency domain. The bone conduction signal is almost free of background noise and therefore ideally *noise-cancelled*.



**Figure 1: Signals at a near-end noise canceller** 

<span id="page-6-0"></span>[Figure 1](#page-5-0) illustrates the signals received at a noise canceller. When a bone conduction signal is provided, the separation of near-end speech and impairing signals can be much improved. The noise canceller's background noise estimation can be improved if a clear separation is possible between speech, speech plus noise and noise only. In the presence of speech, the separation between noise and speech is difficult. The noise canceller may diverge, the speech signal may get degraded. When being able to exactly distinguish between speech and noise based on bone conduction signal, the adaptation control can be improved, e.g. adaptation could be frozen or reduced in adaptation speed and the divergence of the noise canceller may be minimized. Consequently, a high-quality speech signal could be provided in conjunction with low background noise. In general, a similar behaviour can be expected with concurrent talkers. If purely the talker wearing the headsets is transmitted, the concurrent talker can be treated like background noise.

Another improvement with bone conduction sensing can be expected in the double talk situation. In almost any communication device, echo cancellation is used to prevent the far-end listener from echo produced at the near-end device. In general, the echo canceller is an adaptive filter modelling the echo path and trying to minimize the echo signal by subtracting the inverse echo signal, as illustrated in Figure 2. The echo canceller may diverge if the impairing near-end speech signal is not reliably detected. The quality of the adaptation control is key, and the better the echo can be separated from the near-end talker signal the better echo cancellation may work in case of double talk. The use of the bone conduction signal may improve this separation since this represents purely the near-end speech signal.



**Figure 2: The principal functionality of an echo-canceller and associated signals** 

### 5 Measuring human bone conduction signal

### 5.1 Overview

The first step in testing headsets with built-in bone conduction sensors is the understanding of human bone conduction signal inside the ear at a location, where bone conduction sensors of headsets are typically placed.

### 5.2 Measurement setup

To measure the relation between human air-borne signal and bone conduction signal, an experiment was conducted with 11 female and 24 male subjects. The goal was to measure the individual spectra of the air-borne sound and the voice transmitted through bone conduction. The measurements provided an overview of the spread of the individual differences and were the basis for deriving average transfer functions.

<span id="page-7-0"></span>The air-borne speech signal was captured using a free field microphone at the MRP of each test person. For assessing human bone conduction instrumentally, a piezoelectric MEMS voice pickup sensor was placed in a mock-up of an inear headset which was worn by the test persons during the measurements. The speech sequence spoken by the test subjects consisted of eight German sentences according to clause B.3.7 of Recommendation ITU-T P.501 [\[i.3\]](#page-4-0), which were repeated three times, having the mock-up mounted on both the left and the right ear. During the second repetition, the test subject applied some pressure on headset to ensure a proper positioning of the headset. The last repetition was used to derive the average transfer functions, but the results showed no significant differences from the first repetition. Figure 3 shows the mock-up of the in-ear headset and the test setup for one individual.



**Figure 3: Left: mock-up of the in-ear headset Right: test setup for measuring human air-borne and bone-conducted speech signals** 

### 5.3 Measurement results

[Figure 4](#page-8-0) shows the magnitude of the average Fourier Transform of the individual bone-conducted speech signal compared to the acoustic signal at MRP. The analysis was performed using  $1/12<sup>th</sup>$  octave band resolution, which is based on a periodogram (Hann window, FFT size of 16K, 66 % overlap). [Figure 5](#page-8-0) illustrates the average of these signals for female and male talkers. [Figure 6](#page-9-0) shows the average transfer function for male and female speakers. The difference is mainly in the frequency range below 300 Hz, where female voices generally do not provide much signal energy due to the higher fundamental frequency. Consequently, the average male spectrum was chosen as the target spectrum for structure-borne signal simulation. Note that due to the insufficient SNR of the sensors that were available at time of the experiment, the bone conduction signal could only be measured reliably up to 1 kHz. The inverse transfer functions which were used to generate the bone conduction signal from an air-borne speech signal can be found in [Annex A](#page-20-0).

<span id="page-8-0"></span>

**Figure 4: Magnitude of average Fourier Transform of air-borne and bone-conducted signal for each test subject** 



**Figure 5: Average magnitude of air-borne and bone-conducted signals for male and female speakers** 

<span id="page-9-0"></span>

**Figure 6: Average transfer functions for male and female speakers** 

### 6 Human bone conduction simulation

The simulation of human bone conduction is realized using a HATS complying with Recommendation ITU-T P.58 [[i.1](#page-4-0)], which is equipped with modified type 4.4 artificial ears according to Recommendation ITU-T P.57 [\[i.2](#page-4-0)]. The modification consists of an actuator, which allows a realistic simulation of the average human bone-conducted sound for the headset under test. The actuator is integrated close to the position in the ear canal, where also the sensor was located (see clause 5.2). To validate the simulation on HATS, the same sensor as described in clause [5](#page-6-0) was used. Figure 7 shows the average spectra of the original and simulated bone-conducted speech signal. It can be seen that the simulation matches the target response within a tolerance of ±3 dB.



**Figure 7: Comparison of simulated and original human average bone-conducted signal** 

### <span id="page-10-0"></span>7 Test signals and test arrangements

### 7.1 Overview

To evaluate the performance of the noise cancellers, specific test sequences were created to show performance differences with and without simulation of bone conduction. Those test sequences include measurements with interference signals and double-talk measurement. An interference signal could be a background noise or a speech signal from a concurrent talker.

For the test sequences defined in this clause, multiple in-ear headsets from various manufacturers were measured. If applicable, different generations of the same headset were tested.





### 7.2 Measurements in the presence of background noise

#### 7.2.1 Overview

Two test sequences were created so that speech and interference signal do not start simultaneously. The speech signal corresponds to the English sentences described in ETSI TS 103 281 [[i.5\]](#page-4-0) and was calibrated to -4,7 dBPa at MRP. The signal was played back via the artificial mouth of the HATS, which was equipped with the bone conduction simulation. Several binaural background noise scenarios were used to simulate noisy environments according to ETSI ES 202 396-1 [[i.4\]](#page-4-0).

#### 7.2.2 Test methods

#### 7.2.2.1 Speech followed by background noise - Sequence A

The first test sequence (denoted as *Sequence A* hereafter) focuses on the potential divergence of the noise canceller which may happen if suddenly a background noise situation occurs. In this situation, the device may not be able to separate speech and noise, resulting in degraded speech and/or insufficiently cancelled noise.

Two analyses were carried out to investigate the performance of the noise canceller in detail, as indicated in [Figure 8:](#page-11-0)

- S-MOS (speech distortion), N-MOS (noise intrusiveness) and G-MOS (overall quality) are calculated according to ETSI TS 103 281 [[i.5\]](#page-4-0) on the signal parts that overlap with the noise.
- The noise spectrum is analysed immediately after the playback of the speech sequence.

<span id="page-11-0"></span>

**Figure 8: Test sequence A and corresponding analysis** 

#### 7.2.2.2 Background noise followed by speech - Sequence B

The focus of the second test is on the potential divergence of the noise canceller, when speech suddenly occurs during the background noise playback (denoted as *Sequence B* hereafter), as illustrated in Figure 9. Here the focus is set to the degradation of the speech signal, as well as on a possible change in noise reduction performance. S-MOS, N-MOS, and G-MOS were calculated for simultaneously active speech and background noise parts.





#### 7.2.3 Measurement results

#### 7.2.3.1 Speech quality analysis - Sequence A

This clause provides the measurement results from clause [7.2.2.1](#page-10-0) based on the MOS values calculated using the method described in ETSI TS 103 281 [[i.5\]](#page-4-0), as shown in Table 2 to [Table 5.](#page-12-0) Improvements in terms of MOS due to the bone conduction simulation are highlighted in orange. The test results for almost all devices show a clear improvement in S-MOS (speech quality) and indicate that a bone conduction sensor can improve noise cancellation in the device by e.g. detecting active/non-active speech more reliably, which results in an improved speech quality in the presence of background noise.





<span id="page-12-0"></span>

Device number								
<b>BGN</b> scenario	Pub		Midsize car 130 km/h		Pub		Midsize car 130 km/h	
<b>Structure-Borne</b>	Off	On	Off	On	Off	On	Off	On
<b>S-MOS</b>	2,3	2,6	3,6	3,4	2,6	3,2	3,3	3,6
<b>N-MOS</b>	2,9	3,0	3,5	3,8	3,5	3,7	3,9	3,9
<b>G-MOS</b>	.8	2,0	2.	3,0	2,2	2,7	2,9	3,2
Average SNR [dB]	2,81	7,34	12,98	26,47	6,72	18,22	22,16	23,03

**Table 3: MOS results for device 3 and 4, test sequence A** 

#### **Table 4: MOS results for device 5 and 6, test sequence A**



#### **Table 5: MOS results for device 7 and 8, test sequence A**



#### <span id="page-13-0"></span>7.2.3.2 Noise spectrum analysis - Sequence A

This clause illustrates the noise spectra calculated according to clause [7.2.2.1](#page-10-0) for different test devices. The spectra were calculated using a Hann window, FFT size of 16K, and 66 % overlap. A 1/12<sup>th</sup> octave smoothing was applied to the resulted spectra. In [Figure 10](#page-14-0) and [Figure 11,](#page-15-0) it can be noticed that devices 1, 2, and 5 seem to use the information provided from the bone conduction simulation in order to attenuate the background noise transmitted in the uplink after speech is stopped. The attenuation in device 1 takes place in the frequency range up to 500 Hz, whereas devices 2 and 5 attenuate the noise across the whole frequency range. Other devices do not utilize the bone-conducted speech signal and probably apply noise reduction based on the air-borne signal. This is the reason why there is no such difference in the noise spectrum when simulating the human bone conduction speech.

<span id="page-14-0"></span>

**Figure 10: Noise spectrum in uplink with and without bone conduction simulation BGN: Pub** 

<span id="page-15-0"></span>

**Figure 11: Noise spectrum in uplink with and without bone conduction simulation BGN: Midsize Car 130 km/h** 

#### <span id="page-16-0"></span>7.2.3.3 Speech quality analysis - Sequence B

In this clause, results from clause [7.2.2.2](#page-11-0) are provided in Table 6 to Table 9. The performance of the device under test in noisy environment is evaluated with and without bone conduction simulation. Similar to the results in clause [7.2.3.1,](#page-11-0) improvements can be noticed in MOS values with bone conduction simulation, which indicates that these devices benefit from the simulated bone conduction signal to improve the speech quality in noisy environments.

#### **Table 6: MOS results for device 1 and 2, test sequence B**



#### **Table 7: MOS results for device 3 and 4, test sequence B**



#### **Table 8: MOS results for device 5 and 6, test sequence B**



#### **Table 9: MOS results for device 7 and 8, test sequence B**



### <span id="page-17-0"></span>7.3 Double talk measurements

#### 7.3.1 Test method

For double talk testing, the double talk speech test signal from Recommendation ITU-T P.501 [[i.3\]](#page-4-0) is used, as shown in Figure 12. The attenuation range in double talk as described in Recommendation ITU-T P.502 [[i.6\]](#page-4-0) is calculated. The detailed level vs. time analysis of the double talk signal allows a detailed investigation of potential improvement of the double talk performance with bone conduction functionality. The signal of the competing speaker (upper part of Figure 12) is used for the mouth playback.



**Figure 12: Double-talk speech sequence from Recommendation ITU-T P.501 [\[i.3](#page-4-0)]** 

#### 7.3.2 Measurement results

The double talk attenuation for each device is illustrated in [Figure 13.](#page-18-0) Although the attenuation in sending in double talk is already quite low for most devices, it can be seen, that with the use of structure borne, these headsets are more precise in the detection of the send signal and introduce even less attenuation. The attenuation graph with bone conduction simulation active (orange) shows even less attenuation and an almost transparent behaviour of the headset in this double talk situation.

<span id="page-18-0"></span>

**Figure 13: Comparison of double talk attenuation in send direction with and without bone conduction simulation** 

### <span id="page-19-0"></span>8 Conclusion

The present document presents a new method for testing in-ear headset devices which utilize bone conduction sensing and identifies new test sequences to evaluate the performance of noise canceller. The conducted experiments resulted in the following main findings:

- The actual performance of DUTs featuring bone conduction sensors may be significantly degraded when testing without bone conduction simulation.
- Most DUTs rely strongly on the information provided to its bone conduction sensor to detect speech and allow a better control of the noise canceller.
- When measured with bone conduction simulation, speech quality and noise reduction were improved in the uplink for almost all test devices. Devices with bone conduction sensors can be tested and optimized more reliably in a lab where it is possible to fine-tune the noise cancelling algorithms thus optimizing their utilization.
- Most of tested DUTs already have a low double talk attenuation in send direction. However, some headsets were more precise and introduced less attenuation in the uplink signal when simulating the bone conduction signal.
- The results indicate that it is beneficial to simulate the human bone conduction signal when measuring headsets, regardless of whether they are actually equipped with an appropriate bone conduction sensor. For devices not providing this functionality, performance is not further affected.

### <span id="page-20-0"></span>Annex A: Inverse transfer functions

Figure A.1 shows the inverse of the average transfer functions illustrated in [Figure 6.](#page-9-0) These transfer functions can be used to convert a human air-borne speech signal into its corresponding bone conduction signal. Due to the insufficient SNR of the sensors that were available at the time of the experiment, the bone conduction signal could only be measured reliably in the frequency range between 100 Hz and 1 000 Hz. Thus, when using these transfer functions, it is assumed to have a behaviour similar to a bandpass outside this frequency range.



**Figure A.1: Inverse average transfer functions for female and male speakers** 

The magnitudes of both transfer functions in 1/12<sup>th</sup> octave bands between 100 Hz and 1 000 Hz can be found in [Table](#page-21-0) A.1.

<span id="page-21-0"></span>

## <span id="page-22-0"></span>**History**

